

Communication

Sensitivity enhancement in ^{13}C solid-state NMR of protein microcrystals by use of paramagnetic metal ions for optimizing ^1H T_1 relaxation

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Abstract

We discuss a simple approach to enhance sensitivity for ^{13}C high-resolution solid-state NMR for proteins in microcrystals by reducing ^1H T_1 relaxation times with paramagnetic relaxation reagents. It was shown that ^1H T_1 values can be reduced from 0.4–0.8 s to 60–70 ms for ubiquitin and lysozyme in D_2O in the presence of 10 mM $\text{Cu}(\text{II})\text{Na}_2\text{EDTA}$ without substantial degradation of the resolution in ^{13}C CPMAS spectra. Faster signal accumulation using the shorter ^1H T_1 attained by paramagnetic doping provided sensitivity enhancements of 1.4–2.9 for these proteins, reducing the experimental time for a given signal-to-noise ratio by a factor of 2.0–8.4. This approach presented here is likely to be applicable to various other proteins in order to enhance sensitivity in ^{13}C high-resolution solid-state NMR spectroscopy.

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1. Introduction

Over the past years, significant progress has been achieved in solid-state NMR (SSNMR) spectroscopy of biomolecules such as peptides and proteins [1–16]. Particularly, use of protein micro-/nanocrystals [17] has significantly improved resolution in high-resolution SSNMR of dilute spins such as ^{13}C and ^{15}N , permitting signal assignment and structural determination of various uniformly ^{13}C and/or ^{15}N -labeled proteins by SSNMR [18–25]. However, restricted sensitivity in ^{13}C and ^{15}N SSNMR has been still one of the major limiting factors in SSNMR analysis of proteins. In an experimental time required for ^{13}C SSNMR of proteins, more than 95% is typically consumed for recycle delays to retrieve spin polarization by ^1H T_1 relaxa-

tion, to protect a probe from arcing due to RF irradiation, or to avoid sample degradation due to heating. The latter two problems have been addressed by improving designs of MAS probes to minimize sample heating [26] and tolerate handling of relatively high RF power [27], or by using low-power ^1H decoupling [28,29]. Doping with paramagnetic metal ions such as $\text{Cu}(\text{II})$ has been utilized to reduce ^1H T_1 relaxation times in ^{13}C CPMAS of proteins/peptides in cryogenic conditions [30]. However, the effects of paramagnetic doping on resolution and T_1 relaxation have not been fully examined for biomolecular SSNMR, in particular, for ^{13}C CPMAS of protein microcrystals, which generally provides excellent resolution.

In this study, we experimentally investigate the effects of paramagnetic ion doping to reduce ^1H T_1 values in 1D ^{13}C CPMAS for microcrystals of two model proteins: ubiquitin and lysozyme using a $\text{Cu}(\text{II})\text{Na}_2\text{EDTA}$ complex (Cu –EDTA) as a relaxation reagent. In addition to ^1H T_1

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values, we examine resolution and line positions in ^{13}C CPMAS spectra for these proteins in the presence of Cu–EDTA. Motivations and prospects of this approach for sensitivity enhancements in biomolecular SSNMR are presented.

2. Materials and methods

D_2O was purchased from Cambridge isotope (Andover, MA). Ubiquitin from bovine red blood cells (ubiquitin), lysozyme from chicken egg white (lysozyme), and other chemicals were purchased from Sigma–Aldrich (St. Louis, MO). Purified water (double deionized and distilled) was prepared using a High-Q 103 S water still system (High-Q Corp., Wilmette, IL). The purified water was used for preparation of all the protein microcrystals in H_2O .

We prepared protein microcrystals in D_2O or H_2O following the protocols by Martin and Zilm for preparing protein nanocrystals [17] with minor modifications. Unless otherwise mentioned, all the data were collected for samples prepared in D_2O for potential applications to partially deuterated proteins in D_2O . As will be discussed, protein microcrystals prepared in D_2O have longer ^1H T_1 values than those in H_2O . Thus, the effects of paramagnetic doping are more notable for proteins in D_2O , although this approach is also effective for samples prepared in H_2O . An equal volume mixture of a protein stock solution (25 mg protein/ml) and a crystallization solution was concentrated to approximately half the starting volume by using a SpeedVac concentrator (Savant, Farmingdale, NY) [17]. For preparation of the protein stock solution, lysozyme was dissolved in a 100 mM sodium acetate buffer (pH 4.5) while ubiquitin was dissolved in pure $\text{D}_2\text{O}/\text{H}_2\text{O}$. The crystallization solution for ubiquitin contained 25% w/v PEG 8000 and 200 mM cadmium acetate in a 50 mM sodium Hepes buffer (pH 7); the solution for lysozyme contained 12.5% w/v PEG 2000 and 75 mM sodium chloride in a 100 mM sodium acetate buffer (pH 4.5). The concentrated protein solution of ~ 0.5 mL was kept in a microtube at 4°C for 10–12 h to produce protein crystals. Then, the solution containing crystals was centrifuged at 1.5×10^3 g for 5 min using an Eppendorf 5414D micro-centrifuge (Eppendorf, Westbury, NY).

A Cu–EDTA complex was selected as a relaxation reagent that minimizes undesired interactions between metal ions and proteins [31]. To prepare protein crystal samples containing Cu–EDTA, about 0.4 mL of the mother liquor was separated as a supernatant from the protein crystals after the centrifugation. Then, 1.0–14.9 mg of Cu–EDTA was dissolved in the mother liquor. This solution was kept at 4°C for 2–4 h, and centrifuged to remove any precipitated proteins due to the salts. After the pH was adjusted to an appropriate value for the particular protein, the mother liquor containing Cu–EDTA was reintroduced to the protein crystals, and left at 4°C for another 10–12 h to dope Cu–EDTA into protein crystals. The samples which do not contain Cu–EDTA were prepared in the same manner

for a control, but without the addition of Cu–EDTA. Then, the sample was centrifuged for 5 min, and the collected protein crystals were packed into a MAS rotor by centrifugation. The concentration of Cu–EDTA was estimated from the amount of Cu–EDTA used and the total volume of the mother liquor and the protein microcrystals. Formation of the protein crystals were confirmed under an optical microscope. The images of the crystals were obtained at $32\times$ magnification using a CCD camera (Cool-Snap, Roper, Trenton, NJ) attached to a Carl Zeiss Axiovert 25 inverted microscope (Carl Zeiss MicroImaging, Thornwood, NY).

SSNMR experiments were performed at 9.4 T (^1H NMR frequency of 400.2 MHz) with a Varian InfinityPlus 400 NMR spectrometer. For experiments at the spinning speed of 10 kHz, a Varian T3 3.2-mm MAS double-resonance NMR probe or a home-built 2.5-mm MAS double-resonance probe was used. The signals were collected during an acquisition period of 10 ms at the spinning speed of $10,000 \pm 5$ Hz with cooling air at -10°C supplied through a Varian VT stack at a flow rate of ~ 140 standard-cubic-feet per hour (scfh). For experiments at the spinning speed of 40 kHz, we used a 2.0-mm MAS double-resonance probe developed in Dr. Samoson's lab [32–34]. Unless otherwise mentioned, the signals were collected during an acquisition period of 20 ms at the spinning speed of $40,000 \pm 10$ Hz with cooling air at -5°C supplied through the Varian VT stack at a flow rate of ~ 140 scfh and cooled bearing air (1°C). The data were processed with Varian Spinsight software. The spectra in Fig. 2 were processed with Gaussian line broadening of 15 Hz; other spectra were processed with Gaussian line broadening of 25 Hz. ^1H T_1 values were calculated from the data collected by ^1H inversion recovery experiments detected by ^{13}C CPMAS, where a π -pulse to ^1H spins and the following inversion recovery delay were added prior to the conventional CPMAS sequence with ramped CP [35] and TPPM decoupling [36]. The signal intensities were measured for the highest signals in the ^{13}CO (160–190 ppm), $^{13}\text{C}\alpha$ (40–65 ppm), $^{13}\text{CH}_3$ (10–30 ppm) regions to estimate ^1H T_1 ; the average of the ^1H T_1 values estimated for the three regions was used as ^1H T_1 of the sample. For proteins without Cu–EDTA, some variations in ^1H T_1 values ($\sim 10\%$) were observed from batch to batch. We also noticed that ^1H T_1 is gradually reduced (10–25%) over the course of experiments after a week for the proteins without Cu–EDTA. The values for ^1H T_1 in Table 1 were measured within a week after the sample was packed in a rotor.

3. Results and discussion

In Fig. 1(a)–(d), we demonstrate sensitivity enhancements in ^{13}C CPMAS by faster signal accumulation using short ^1H T_1 optimized with Cu–EDTA doping for (a and b) lysozyme and (c and d) ubiquitin microcrystals. These spectra were collected (a and c) with 10 mM Cu–EDTA and (b and d) without Cu–EDTA in a common experimen-

Table 1
 ^1H T_1 values of ubiquitin and lysozyme in the presence and absence of Cu–EDTA with their approximate crystal sizes measured from microscopic images

Protein	Crystal size (μm)	^1H $T_1^{\text{D}_2\text{O}}$ (ms) ^a	^1H $T_1^{\text{H}_2\text{O}}$ (ms) ^b	With Cu–EDTA in D_2O	
				[Cu–EDTA] (mM)	^1H T_1 (ms) ^c
Ubiquitin	1–5	820 ± 10	307 ± 19	10	73 ± 1
Lysozyme	5–20	350 ± 4	280 ± 5	10	59 ± 1

^a ^1H T_1 for the sample prepared in D_2O used for Figs. 1(b and d). ^1H T_1 values were 500 and 820 ms for Fig. 2(b), (d), respectively.

^b ^1H T_1 for the sample prepared in H_2O .

^c ^1H T_1 for the sample used for Fig. 1(a and c). ^1H T_1 values were 60 ms for both Fig. 2(a) and (c).

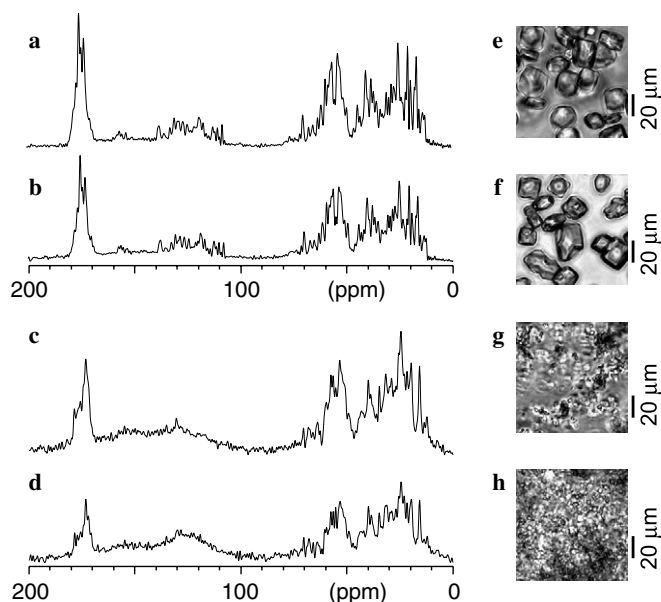


Fig. 1. (a–d) ^{13}C CPMAS spectra of protein crystals for (a and b) lysozyme and (c and d) ubiquitin prepared in D_2O obtained (a and c) with and (b and d) without 10 mM Cu–EDTA at a ^{13}C NMR frequency of 100.6 MHz. The recycle delays were set to (a) 0.5 s, (b) 1.1 s, (c) 1.0 s, and (d) 2.5 s. The spectra were acquired at a spinning speed of 10 kHz under ^1H TPPM decoupling of (a and b) 71 kHz and (c and d) 90 kHz. Signals were accumulated during acquisition periods of 10 ms with (a) 28,160, (b) 12,800, (c) 14,336, and (d) 5736 scans in a common total experimental time of 4 h. During the CP period of 1.0 ms, ^{13}C RF field was swept (a and b) from 56 to 76 kHz and (c and d) from 52 to 72 kHz, while ^1H RF field was kept at (a and b) 76 kHz and (c and d) 72 kHz. All the spectra were processed with Gaussian line broadening of 25 Hz. At the right of the spectra in (a)–(d), microscope images of the corresponding protein micro-/nanocrystals used for the NMR experiments are displayed in (e)–(h). The images were obtained at 32 \times magnification.

tal time of 4 h. Inspections of the microscopic images in Fig. 1(e)–(h) for the crystals (e and g) with and (f and h) without Cu–EDTA revealed that there were no noticeable changes in the crystal shapes or sizes due to the introduction of Cu–EDTA for (e and f) lysozyme and (g and h) ubiquitin. Hence, it is not likely that the addition of Cu–EDTA damaged the protein crystals. The recycle delays for the lysozyme samples were (a) 0.5 s (^1H $T_1 = 59$ ms) and (b) 1.1 s (^1H $T_1 = 350$ ms) while the delays for the ubiquitin samples were (c) 1.0 s (^1H $T_1 = 73$ ms) and (d) 2.5 s (^1H $T_1 = 820$ ms). As will be discussed later, increasing the Cu–EDTA concentration further reduces ^1H T_1

values. For comparison, the spectra were scaled so that the spectra for the same protein display a common noise level. Faster signal accumulation using the shorter ^1H T_1 in the presence of Cu–EDTA clearly yielded considerable sensitivity enhancements by factors of 1.4 and 1.6 in Fig. 1(a) and (c), respectively. It is also clear that no major changes in the line positions or line-widths were induced by the presence of 10 mM Cu–EDTA. Since line positions in ^{13}C CPMAS spectra were not altered by the Cu–EDTA doping, major structural changes in the proteins due to Cu–EDTA doping are not likely. ^1H T_1 values were successfully reduced by a factor of 6–11. On the other hand, we were able to speed up the experiment by only up to 2.5 times to protect a probe from arcing under high-power ^1H RF decoupling. We also tested decoupling by fast MAS at 20–30 kHz, which was successfully employed in our recent studies for paramagnetic systems [37–39]. However, the resolution without ^1H RF decoupling is considerably limited for the diamagnetic poly-crystalline proteins.

To overcome this problem, we employed a rotor-synchronous π -pulse train decoupling under ultra-fast MAS condition (40 kHz), which was recently proposed by Hafner and coworkers at Varian [40]. We found that this decoupling permits narrowing comparable to TPPM decoupling of ^1H RF irradiation at 200 kHz under MAS at 40 kHz. An equivalent decoupling sequence was successfully applied for ^1H decoupling for paramagnetic systems [39] and ^{19}F decoupling for fluoro-polymers [41] under fast MAS (≥ 20 kHz). Fig. 2 shows CPMAS spectra at a spinning speed of 40 kHz for (a and b) lysozyme and (c and d) ubiquitin microcrystals (a and c) with and (b and d) without 10 mM Cu–EDTA doping. The recycle delays for the lysozyme samples were (a) 180 ms (^1H $T_1 = 60$ ms) and (b) 1.5 s (^1H $T_1 = 500$ ms) while the delays for the ubiquitin samples were (c) 180 ms (^1H $T_1 = 60$ ms) and (d) 2.5 s (^1H $T_1 = 820$ ms). We confirmed that faster signal accumulation with the low-duty-factor ^1H decoupling sequence at a spinning speed of 40 kHz further enhanced sensitivity in the ^{13}C CPMAS spectra by a factor of 2.7–2.9, which speeds up our experiments seven- to eightfold. The resolution of the CPMAS spectra obtained with fast recycling in the presence of Cu–EDTA was comparable to that without Cu–EDTA. It is noteworthy that the effective RF duty factor due to ^1H decoupling is only $\sim 1.1\%$ in the experiment with a recycle delay of 180 ms and an acquisition period of 20 ms. Because of the low RF duty factor and

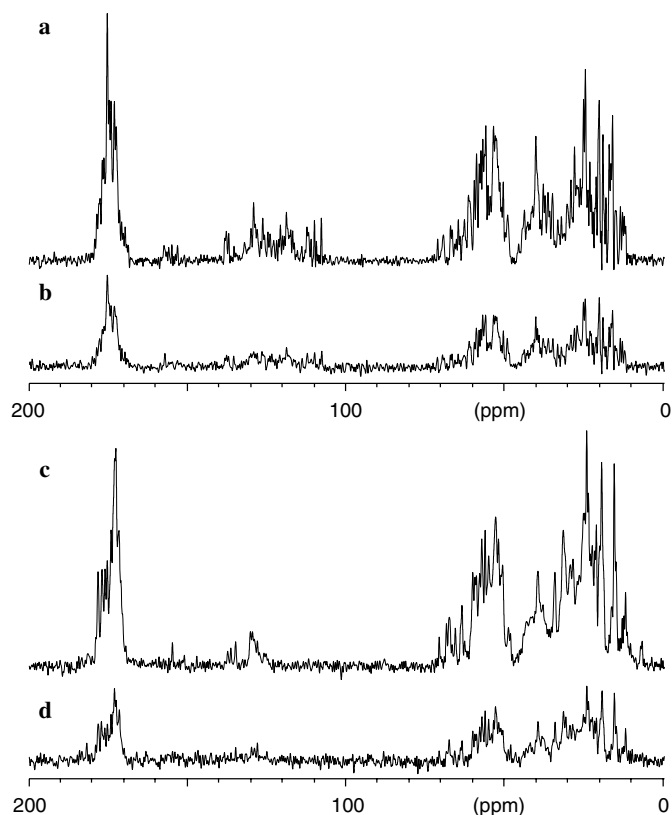


Fig. 2. (a–d) ^{13}C CPMAS spectra of protein microcrystals for (a and b) lysozyme and (c and d) ubiquitin prepared in D_2O obtained (a and c) with and (b and d) without 10 mM Cu–EDTA at a ^{13}C NMR frequency of 100.6 MHz. The recycle delays were (a) 0.18 s, (b) 1.50 s, (c) 0.18 s, and (d) 2.50 s. The spectra were acquired at a spinning speed of 40 kHz with π -pulse-train decoupling. In the decoupling scheme, a π -pulse with the width of 2.5 μs was rotor-synchronously applied at the end of every rotor cycle (25 μs) with the XY-8 phase cycle [51]. Signals were accumulated during acquisition periods of 20 ms with (a) 36,000, (b) 4800, (c) 72,000, and (d) 5680 scans in a common total experimental time of (a and b) 2 h or (c and d) 4 h. During the CP period of 1.0 ms, the ^{13}C RF field was swept from 53 to 71 kHz, while the ^1H RF field was kept at 102 kHz. All the spectra were processed with Gaussian line broadening of 15 Hz.

high efficiency of the ^1H RF circuit of the fast MAS probe, we could collect the signals up to 30 ms of acquisition periods without any arcing problems. Thus, significant sensitivity enhancements with uncompromised resolution in this approach are possible under the fast MAS condition.

We prepared crystals in D_2O and H_2O without Cu–EDTA to examine solvent effects on ^1H T_1 values. Considerably longer ^1H T_1 was observed in D_2O for ubiquitin and, to a lesser degree, for lysozyme, as shown in Table 1. The sensitivity enhancements for the proteins in H_2O are less, particularly for ubiquitin. Nevertheless, considerable sensitivity gains (~ 2) are still expected under the fast MAS and decoupling condition used for Fig. 2. Martin and Zilm reported that ^1H T_1 of unlabeled ubiquitin nanocrystals in H_2O is 0.5 s [17]. Zilm and coworkers more recently reported average ^1H T_1 values of 300–400 ms for uniformly ^2D - and ^{15}N -labeled ubiquitin nanocrystal samples for which amide protons are back-exchanged in H_2O ,

as well as for unlabeled ubiquitin [42]. Thus, the long ^1H T_1 observed for our ubiquitin sample in D_2O cannot be simply explained by lower ^1H density. Understanding this solvent dependence of ^1H T_1 requires more systematic work, and a fuller study is outside of the scope of this study.

Fig. 3 shows ^{13}C CPMAS spectra of ubiquitin microcrystals acquired at different ^1H inversion recovery delays (a) without and (b) with 10 mM Cu–EDTA. This result clearly shows that the ^1H T_1 value of ubiquitin is reduced by the introduction of Cu–EDTA in a uniform manner for different chemical groups and residues. After 50 ms, the ^{13}C CPMAS spectra in (b) display a null signal in the presence of Cu–EDTA, while the spectra in (a) show a signal close to the null only after 800 ms without Cu–EDTA. ^1H T_1 values obtained from the experiments are (a) 830 ms and (b) 73 ms. In a recent study on uniformly ^{13}C -labeled ubiquitin by Igumenova et. al., it has been reported that a 2D $^{13}\text{C}/^{13}\text{C}$ chemical-shift correlation experiment at a ^1H frequency of 800 MHz required about 36 h with recycle delay of 1.5 s [43]. Assuming that the RF-duty factor and the sample stability are not the limiting factor, it is possible to speed up this experiment up to seven times with a shorter ^1H T_1 value of ~ 70 ms in the paramagnetic doping approach.

Fig. 4 shows Cu–EDTA concentration dependence of the longitudinal relaxation rate $1/T_1$ for the lysozyme sample. Fig. 4 clearly demonstrates that $1/T_1$ is not linearly proportional to the concentration of Cu–EDTA. The slope is the largest at the lower Cu–EDTA concentration (5–10 mM). At higher concentration, the relaxation rate increases more slowly for a given increase in the Cu–EDTA concentration. This is probably because ^1H T_1 relaxation due to the paramagnetic reagents is mediated by a ^1H – ^1H spin diffusion mechanism [44]. Since Cu–EDTA is hydrophilic, it is most likely that ^1H polarization is retrieved

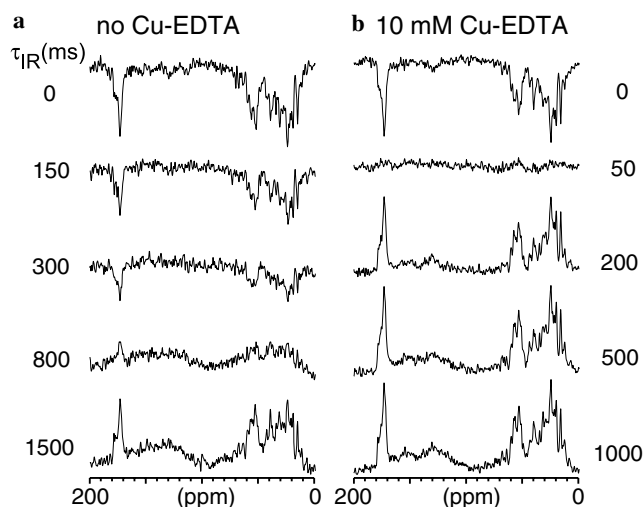


Fig. 3. ^1H inversion recovery delay (τ_{IR}) dependence of ^{13}C CPMAS spectra of ubiquitin microcrystals prepared in D_2O (a) without and (b) with 10 mM Cu–EDTA obtained at 10 kHz MAS. The values of τ_{IR} used in the experiments are indicated in the figure.

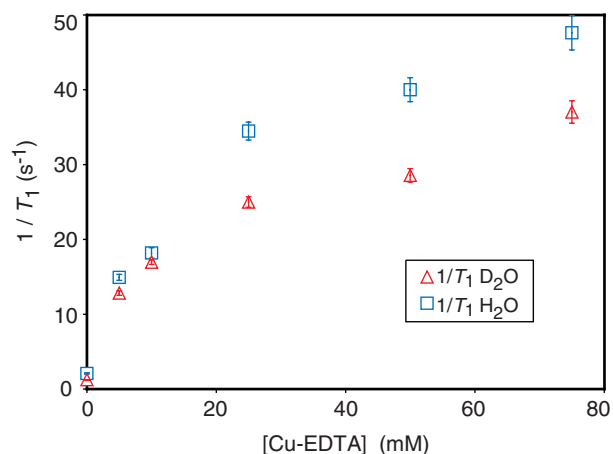


Fig. 4. Cu-EDTA concentration dependence of the ^1H relaxation rate ($1/T_1$) for lysozyme microcrystals prepared in D_2O (triangle) and H_2O (square). The ^1H T_1 values were measured by the inversion recovery experiment shown in Fig. 3. The error bars indicate standard errors in the measurements of $1/T_1$.

more quickly by paramagnetic T_1 relaxation around the water-accessible protein surface, where Cu-EDTA is easily accessible. The recovered polarization can be transferred across the molecule by ^1H - ^1H spin diffusion. We noticed that there is minor solvent dependence of ^1H T_1 even in the presence of Cu-EDTA. Slightly lower ^1H $1/T_1$ rates in D_2O may be attributed to slower ^1H - ^1H spin diffusion in D_2O , in which amide hydrogens are exchanged for ^2D . In spite of the difference, we found that in both H_2O and D_2O solvents, ^1H T_1 for the protein microcrystal samples can be reduced to 20–30 ms in the presence of 75 mM Cu-EDTA.

In Fig. 5, we examined resolution of ^{13}C CPMAS spectra for (a and b) lysozyme and (d and e) ubiquitin microcrystals (a and d) without and (b and e) with 10 mM Cu-EDTA, where only the aliphatic region of the spectra are displayed for clarity. The spectra in (c and f) show the difference between the spectra without and with Cu-EDTA for (c) lysozyme and (f) ubiquitin. As discussed above, in (b and e), no major changes were observed by the addition of 10 mM Cu-EDTA. Although ^1H T_1 values were reduced by factors of (b) 8.3 and (e) 13.7, the line broadening is only subtle (10–20%). However, we observed that a few resonances observed in Fig. 5(a and d) are substantially reduced in intensity in the spectra in (b and e) (indicated by arrows). The quenched signals may be assigned to residues exposed to the protein surface, at which ^{13}C spins can be subject to much faster paramagnetic T_2 relaxation due to Cu-EDTA in water phase. It is known that paramagnetic ^{13}C T_2 relaxation rates are proportional to $1/R^6$, where R is the distance between a ^{13}C spin and a paramagnetic ion [45,46]. Hong et al. reported that the paramagnetic quenching can be utilized to measure distances of ^{13}C sites in membrane bound peptides from the membrane surface with ranging Mn(II) concentration in water phase [46]. Thus, it is probable that signals for residues exposed to the protein surface are selectively quenched by the paramagnetic effects, while the majority of signals for other residues are unaffected. Further studies are needed to examine the possibilities of using the effects for structural analysis. The difference spectra in (c,f) also suggest that the effects of paramagnetic quenching are relatively minor; the integral intensities of (c) and (f) are only 2 and 11% of those for (a) and (d), respectively. Considering that the amount of the proteins may differ by 5–10% be-

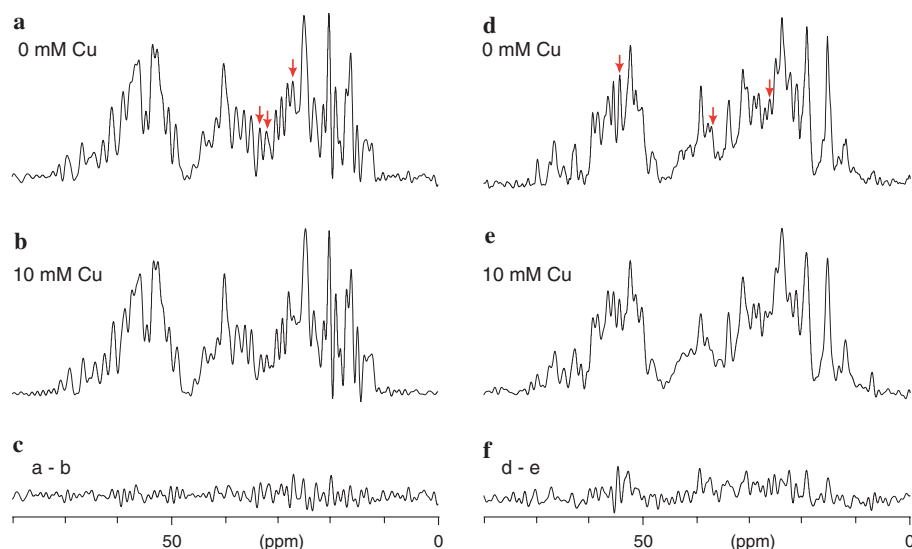


Fig. 5. ^{13}C CPMAS spectra of (a and b) lysozyme and (d and e) ubiquitin protein crystals with Cu-EDTA concentrations of (a and d) 0 mM, (b and e) 10 mM. The spectra in (c and f) are the difference between the spectra obtained with and without Cu-EDTA for the same sample. The spectra were obtained at a ^{13}C NMR frequency of 100.6 MHz at a spinning speed of 40 kHz with ^1H π pulse-train decoupling during the acquisition periods of 10 ms. The shorter acquisition periods were adopted to minimize the noise level for comparison. The recycle delays were (a) 1.50 s, (b) 0.18 s, (d) 2.50 s, and (e) 0.18 s. All the spectra were processed with Gaussian line broadening of 25 Hz.

tween (d) and (e) [or (a) and (b)], the overall signal quenching due to the Cu(II) addition is less than the significant level. We also found that the resolution in ^{13}C CPMAS spectrum of lysozyme was not substantially degraded by the addition of 75 mM Cu–EDTA (data not shown). The ^1H T_1 value in this condition is about 27 ms, which is one tenth of the ^1H T_1 for the same protein without Cu–EDTA. Therefore, for the majority of the signals, further sensitivity enhancement is possible with more optimized pulse sequences for this purpose.

4. Conclusion

In this study, we demonstrated that ^1H T_1 values of the two model proteins, lysozyme and ubiquitin, in microcrystals can be reduced to ~ 60 ms by Cu–EDTA doping without major degradation in the resolution of their ^{13}C CPMAS spectra. We also demonstrated that significant sensitivity enhancements of 1D ^{13}C CPMAS spectra were attained for these proteins by faster signal repetitions using the reduced ^1H T_1 values under fast MAS. Although the full potential of this approach for sensitivity enhancement is still restricted only in the fast MAS condition, our study presented a new opportunity to gain significant sensitivity enhancements using paramagnetic doping in biomolecular SSNMR. In this communication, we focused on testing this approach in 1D ^{13}C CPMAS for unlabeled ubiquitin and lysozyme microcrystals. It is probable that the present approach can be adopted in CPMAS or static experiments of other insoluble proteins. The successful reduction of ^1H T_1 relaxation times in the present experiments will also open new possibilities of sensitivity enhancements in more advanced experiments such as multi-dimensional ^{13}C SSNMR of uniformly ^{13}C -labeled proteins [18–25] and various distance measurements [3,11,13,47–50] for selectively ^{13}C -labeled protein samples in our future studies.

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